

# Mathematical modelling of atherosclerotic plaque formation



## Atherosclerosis

## Mathematical Modelling

## Simulation

## Summary

Atherosclerosis

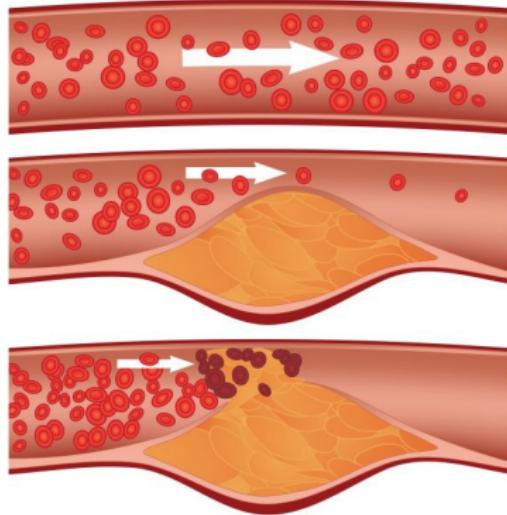
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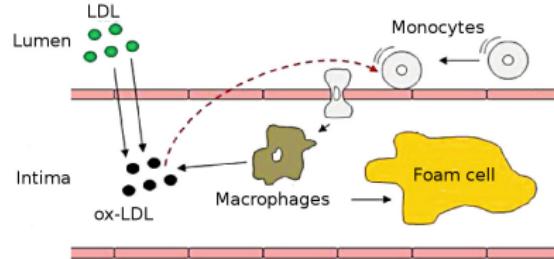
## Atherosclerosis

- ▶ atherosclerosis is an inflammatory process mainly triggered by low-density lipoproteins (LDL)
- ▶ may lead to: occlusion of artery, rupture  
⇒ heart attack, stroke
- ▶ risk factors: blood pressure, age, gender, genetic endowment, smoking...



## Atherosclerosis II

- ▶ LDL penetration/oxidation initiate inflammatory process
- ▶ intima LDL concentration depends on plasma LDL/wall permeability
- ▶ ox. LDL activates endothelial cells which trigger monocyte recruitment
- ▶ monocytes differentiate into active macrophages
- ▶ active macrophages absorb ox. LDL (mass action law)
- ▶ macrophages transform into foam cells
- ▶ foam cells are responsible for local volume increase
- ▶ smooth muscle cells migrate to form fibro-muscular cap



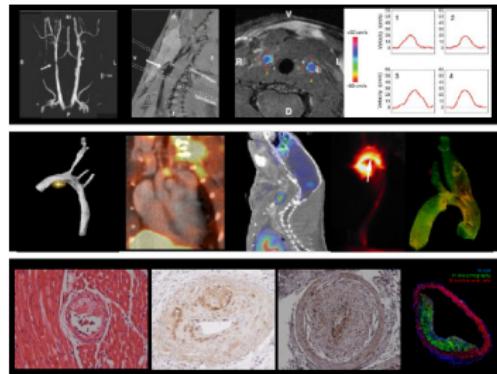
## SFB 656 - Molecular Cardiovascular Imaging



**SFB 656**  
**MoBil**

- ▶ broad investigations in molecular and inflammatory aspects of atherosclerosis through newly developed tracers and methods
- ▶ mouse models

▶ last funding proposal:  
07/2013 – 06/2017

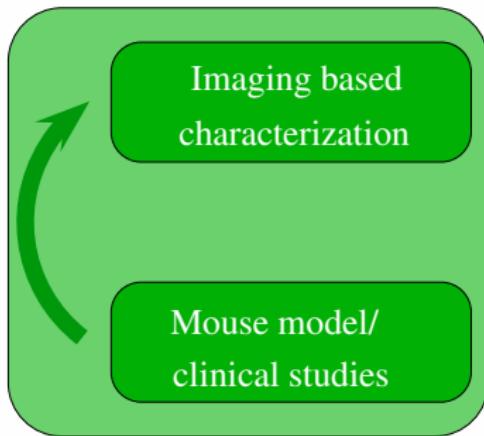


## Project B07

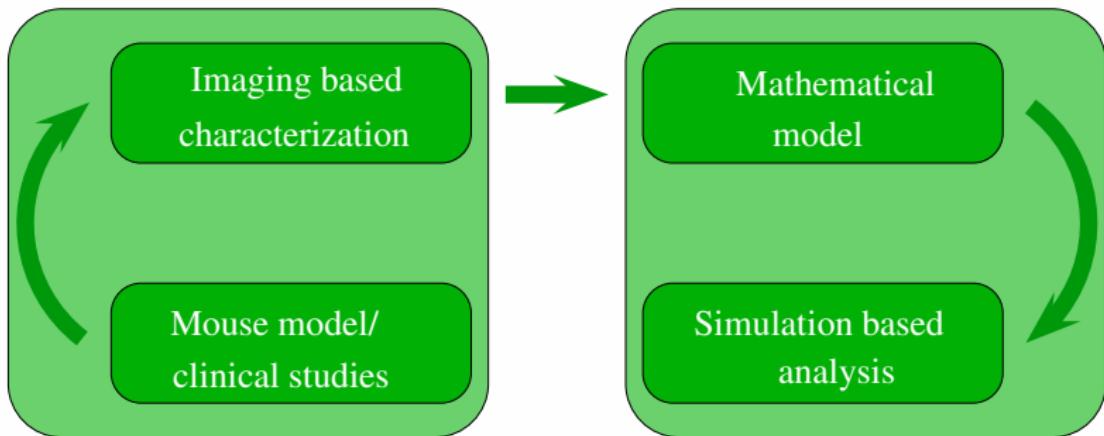


- ▶ Mathematical modelling of atherosclerotic plaque formation based on data from multiparametric imaging
- ▶ principal investigator: Prof. Mario Ohlberger
- ▶ scientific staff: Rene Milk, Stefan Girke
- ▶ co-operation partner: Prof. Christina Surulescu, Prof. Michael Schäfers



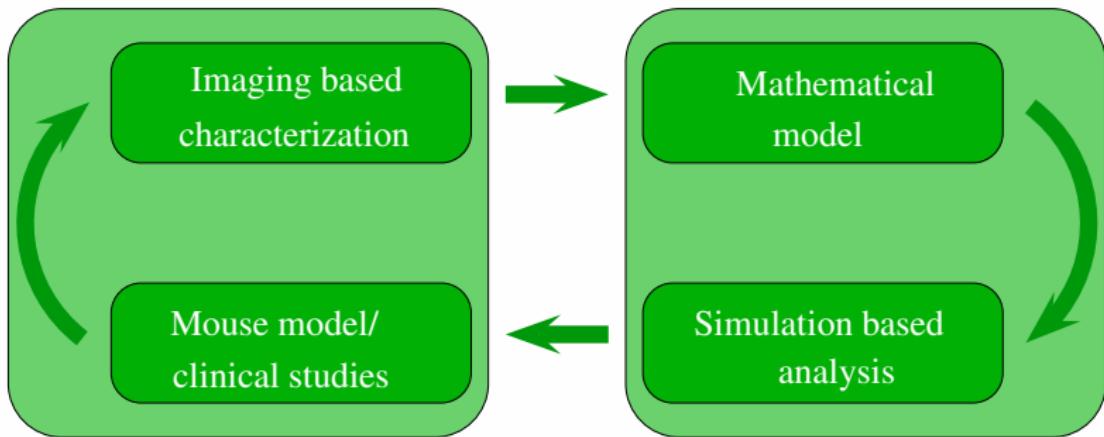


**SFB 656**  
**MoBil**



**SFB 656**  
**MoBil**

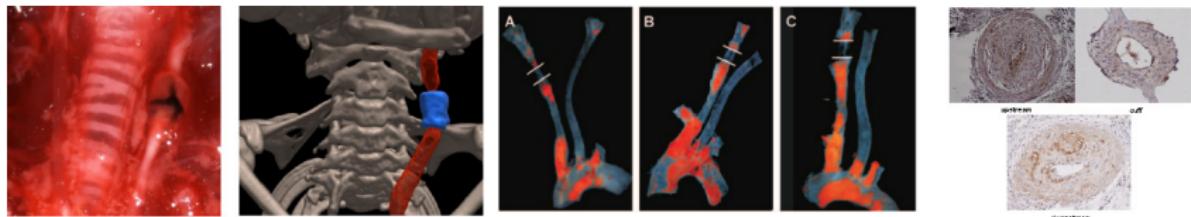




Provide deeper insight into  
plaque progression and stability

## New aspects - wall shear stress

- ▶ penetration of LDL through the endothelial layer is influenced by the blood flow through the wall shear stress



- ▶ all ApoE<sup>-/-</sup> mice with a cuff around right carotid suffered a heart attack after fed with a high cholesterol diet

## New aspects - matrix metalloproteinase

- ▶ matrix metalloproteinase (MMP) helps degrading the extracellular matrix
  - ⇒ restructuring of the lesion
- ▶ it is believed that MMPs contribute to remodelling, by
  - ▶ enabling smooth muscle cells to migrate
    - ⇒ form a fibrous cap
  - ▶ degrading this encapsulation
    - ⇒ mechanical instability, vulnerability of the plaques

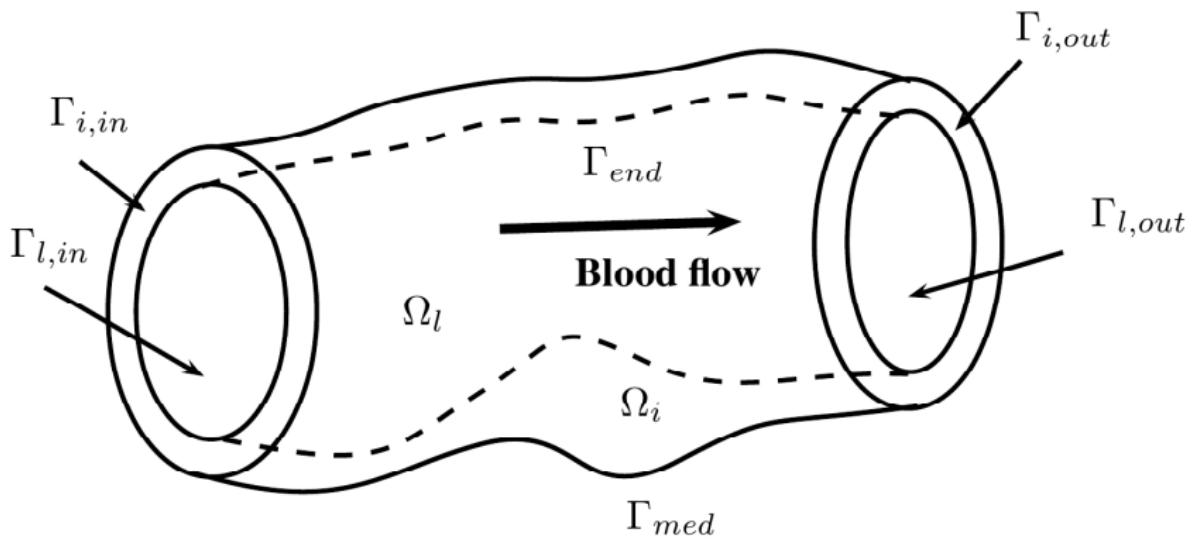
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## Domain



## Overview mathematical model [Calvez2009]

- ▶ Navier-Stokes flow in the lumen
- ▶ Darcy perfusion in the intima
- ▶ reactive transport system for
  - ▶ LDL in the lumen
  - ▶ LDL in the intima
  - ▶ oxidized LDL in the intima
  - ▶ signal
  - ▶ macrophages
  - ▶ foam cells
  - ▶ smooth muscle cells
  - ▶ (matrix metalloproteinase)

## Blood flow [Calvez2009]

lumen (Navier-Stokes)

$$\begin{aligned}
 & \rho[\partial_t u_l + (u_l \cdot \nabla) u_l] - \nu \Delta u_l + \nabla p_l = 0, & x \in \Omega_l, t \in [0, T], \\
 & \nabla \cdot u_l = 0, & x \in \Omega_l, t \in [0, T], \\
 & u_l = U_{l,in}, & x \text{ on } \Gamma_{l,in}, t \in [0, T], \\
 & T(u_l, p_l)n_l = -p_{out}n_l, & x \text{ on } \Gamma_{l,out}, t \in [0, T], \\
 & u_l \cdot n_l = \mathbf{J}_v, & x \text{ on } \Gamma_{end}, t \in [0, T], \\
 & u_l - (u_l \cdot n_l)n_l = 0, & x \text{ on } \Gamma_{end}, t \in [0, T].
 \end{aligned}$$

intima (Darcy)

$$\begin{aligned}
 & u_i = -\frac{K}{\mu} \nabla p_i, & x \in \Omega_i, t \in [0, T], \\
 & \nabla \cdot u_i = 0, & x \in \Omega_i, t \in [0, T], \\
 & u_i \cdot n_i = 0, & x \text{ on } \Gamma_{i,in} \cup \Gamma_{i,out}, t \in [0, T], \\
 & u_i \cdot n_i = -\mathbf{J}_v, & x \text{ on } \Gamma_{end}, t \in [0, T], \\
 & p_i = p_{med}, & x \text{ on } \Gamma_{med}, t \in [0, T].
 \end{aligned}$$

## LDL evolution

lumen

$$\begin{aligned}\partial_t c_l + \nabla \cdot (-D_l \nabla c_l + u_l c_l) &= 0, & x \in \Omega_l, t \in [0, T], \\ c_l &= C_{l,in}, & x \text{ on } \Gamma_{l,in}, t \in [0, T], \\ \nabla c_l \cdot n_l &= 0, & x \text{ on } \Gamma_{l,out}, t \in [0, T], \\ (-D_l \nabla c_l + u_l c_l) \cdot n_l &= \mathbf{J}_s, & x \text{ on } \Gamma_{end}, t \in [0, T].\end{aligned}$$

intima

$$\begin{aligned}\partial_t c_i + \nabla \cdot (-D_i \nabla c_i + u_i c_i) &= -r_{ox} c_i, & x \in \Omega_i, t \in [0, T], \\ \nabla c_i \cdot n_i &= 0, & x \text{ on } \Gamma_{i,in} \cup \Gamma_{i,out} \cup \Gamma_{med}, t \in [0, T], \\ (-D_i \nabla c_i + u_i c_i) \cdot n_i &= -\mathbf{J}_s, & x \text{ on } \Gamma_{end}, t \in [0, T].\end{aligned}$$

## Coupling of blood flow and LDL evolution

Kedem-Katchalsky equations  
(flux through semipermeable membrane)

$$\begin{aligned} J_v &= L_p ([p_l - p_i] - \alpha [c_l - c_i]), \\ J_s &= \xi ([c_l - c_i] - \beta J_v) \end{aligned}$$

⇒ simplification

$$\begin{aligned} J_v &= L_p (p_l - p_i), \\ J_s &= \xi (c_l - c_i) \end{aligned}$$

## Inflammatory process

### Plaque growth

$$\begin{aligned} -\nabla \cdot D(v) + \nabla q = 0, \quad & \nabla \cdot v = \frac{k_F}{A} c_{ox} \cdot M & x \in \Omega_i, t \in [0, T], \\ -D(v)n_i u - q n_i = 0, & & x \text{ on } \Gamma_{end}, t \in [0, T], \\ v = 0, & & x \text{ on } \partial\Omega_i \setminus \Gamma_{end}, t \in [0, T]. \end{aligned}$$

### oxidized LDL

$$\begin{aligned} \partial_t c_{ox} = d_{ox} \Delta c_{ox} - k_F c_{ox} \cdot M + r_{ox} c_i, & x \in \Omega_i, t \in [0, T], \\ \partial_{n_i} c_{ox} = 0, & x \text{ on } \partial\Omega_i, t \in [0, T]. \end{aligned}$$

### macrophage

$$\begin{aligned} \partial_t M = d_M \Delta M - k_F c_{ox} \cdot M, & x \in \Omega_i, t \in [0, T], \\ \partial_{n_i} M = -f(S), & x \text{ on } \Gamma_{end}, t \in [0, T], \\ \partial_{n_i} M = 0, & x \text{ on } \partial\Omega_i \setminus \Gamma_{end}, t \in [0, T]. \end{aligned}$$

### signal

$$\begin{aligned} \partial_t S = d_S \Delta S - \lambda S + \gamma(c_{ox} - c_{ox}^{\text{th}})_+ + k_F c_{ox} \cdot M, & x \in \Omega_i, t \in [0, T], \\ \partial_{n_i} S = 0, & x \text{ on } \partial\Omega_i, t \in [0, T]. \end{aligned}$$

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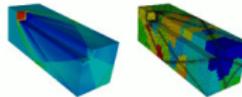
# Implementation



Distributed and Unified Numerics Environment

Distributed and Unified Numerics Environment

- ▶ Dune 2.2.1-release and Dune-Fem 1.3-release
- ▶ implementation is based on code from fuel cell project



[Steinkamp2008]

- ▶ using LDG passes [Burri2006]  
(example:  $\mathcal{L} = \Delta = \nabla \cdot (\nabla) = \mathcal{L}_{\text{post}} \circ \mathcal{L}_2 \circ \mathcal{L}_1 \circ \mathcal{L}_{\text{pre}}$ )

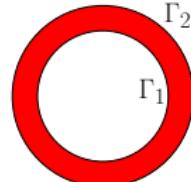
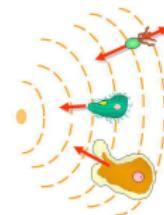
## Inflammation, 3 species, intima [Ibragimov2005]

$$\partial_t n_1 = \mu_1 \Delta n_1 - \underbrace{\chi_{11}^0 \nabla \cdot \left( \frac{n_1}{c_1} \nabla c_1 \right)}_{\text{chemotaxis}},$$

$$\partial_t n_3 = \mu_3 \Delta n_3 + \underbrace{F_0 n_1 n_3}_{\text{dying immune cells increase debris}},$$

$$\partial_t c_1 = \nu_1 \Delta c_1 - \underbrace{\alpha_1 n_1 c_1}_{\text{immune cells dec. signal}} + \underbrace{\gamma n_3}_{\text{debris prod. signal}}$$

- ▶  $n_1$  = immune cells (i.e. macrophages...),
- ▶  $n_3$  = debris (i.e. foam cells...),
- ▶  $c_1$  = signal



## Boundary data

no inflow, except:

- ▶ immune cells are triggered and enter intima through the inner boundary, if a threshold is reached

$$\partial_\eta n_1 = \begin{cases} \beta_1, & c_1(x) > c_1^*, \\ 0, & \text{else} \end{cases}, \quad x \in \Gamma_1,$$

$$\partial_\eta n_1 = 0, \quad x \in \Gamma_2,$$

$$\partial_\eta n_3 = 0, \quad x \in \Gamma_i, i = 1, 2,$$

$$\partial_\eta c_1 = 0, \quad x \in \Gamma_i, i = 1, 2$$

## Initial data

- ▶ immune cells are more likely near the inner boundary
- ▶ debris is seeded at a point  $x_0$
- ▶ signal with constant distribution

$$n_1^0(x) = \varepsilon_1 \exp(-Q_1|r_1^2 - \|x\|_2^2|),$$

$$n_3^0(x) = \varepsilon_2 \exp(-Q_2\|x_0 - x\|_2^2),$$

$$c_1^0(x) = \varepsilon_3$$



## Discretization

- ▶ Local Discontinuous Galerkin
- ▶ polynomial order 1
- ▶ explicit euler scheme
- ▶ adaptivity



start movie cross section



## Inflammation in a cuff model (3D)

start movie cuff 3D

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## Further implementation

- ▶ (semi) implicit solvers
- ▶ parallelization
- ▶ solving whole system
- ▶ different time scales
- ▶ more dofs
- ▶ real data

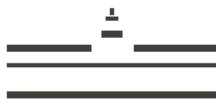


## Project outline

- ▶ efficient numerical model for atherogenesis
- ▶ usage of imaging derived parameters
- ▶ analysis of the influence of local blood flow dynamics on plaque formation
- ▶ modelling of macrophages and the production of MMPs in the context of lesion restructuring
- ▶ simulation based analysis for a well defined mouse model

## References

-  [Calvez2009] Calvez, V. et al,  
Mathematical modelling of the atherosclerotic plaque formation.  
*ESAIM Proceedings* 28:1–12, 2009
-  [Ibragimov2005] Ibragimov, A.I. et al,  
A mathematical model of atherogenesis as an inflammatory response  
*Mathematical Medicine and Biology* 22(4):305–333, 2005
-  [Steinkamp2008] Steinkamp, K. et al,  
A non-isothermal PEM fuel cell model including two water transport mechanisms in the  
membrane  
*ASME J. Fuel Cell Sci. Technol.* 5(1):011007, 2008
-  [Burri2006] Burri, A. et al  
A general object oriented framework for discretizing non-linear evolution equations  
*Springer Advances in High Performance Computing and Computational Sciences*:69–87,  
2006



# Thank you for your attention!